Laryngeal Biomechanics: An Overview of Mucosal Wave Mechanics

Gerald S. Berke and Bruce R. Gerratt

Head and Neck Surgery, University of California at Los Angeles, and VA Medical Center, West Los Angeles, Los Angeles, California, U.S.A.

Summary: The biomechanics of wave propagation in viscoelastic materials can be useful in understanding the nature of normal and pathologic vocal fold vibration. Mucosal wave movement is the primary means by which the larynx transforms the egressive pulmonary air flow into sound. This short tutorial describes a number of concepts fundamental to the understanding of the vocal fold traveling wave. The displacement velocity of the vocal folds is shown to be proportional to the wave speed, which in turn is proportional to the elastic modulus or stiffness of the vocal folds. Finally, a few cases of unilateral paralysis are used to demonstrate how vocal fold stiffness, entrainment, and degree of vocal fold closure interact to create the complex vibratory patterns that occur in disordered laryngeal states. It is emphasized that surgical voice restoration must consider these properties of the mucosal wave to improve phonatory function. Key Words: Larynx—Mucosal wave movement—Phonation—Voice.

For many years, it has been known that a fundamental element of vocal fold vibration is the mucosal wave (1). However, its significance in the process of diagnosing and treating laryngeal disorders is one of the most neglected aspects of laryngology and speech pathology. A greater understanding of the vocal fold traveling wave will lead to an increased awareness of the biomechanics of vocal production and its role in procedures used to improve voice.

BASICS OF VOCAL FOLD VIBRATION

After the closure of the glottis, the pulmonary-generated air flow directed between the apposed vocal folds causes them to vibrate (2). The forces acting on the folds that sustain self-oscillation are not well understood (see Titze, 1980, for example) (3,4). Nevertheless, vibration of the vocal folds is characterized by a tissue wave with compressive and rarefactive phases. The laryngeal tissue wave modulates the air stream flowing through the glottis into a series of puffs (or pulses) of air released into the vocal tract. The physical properties of these released air puffs are the critical elements in the acoustic properties of the sound produced (5).

The delay between the compression and rarefaction of the tissue wave as it travels the vertical extent of the vocal folds produces a “phase difference” between the opening and closing of the inferior and superior portions of the vocal folds (6). Figure 1A, B, and C are high-speed photographic images of the vibrating vocal folds in an in vivo canine model. Figure 1A shows the glottis in its most open configuration, in which the upper and lower margins are at the same displacement amplitude (i.e., distance from the midline). Figure 1B, slightly further into the cycle, shows the continued compression of the upper margin of the vocal folds, while rarefaction is seen as the lower margins’ re-
FIG. 1. A: High-speed photographic image of a vibrating glottis in an in vivo canine model during the most open portion of the cycle. Note that the lower and upper margins are at the same displacement. B: High-speed photographic image of a vibrating glottis in an in vivo canine model during the closing phase. Note the difference in displacement between the lower and upper margins. C: High-speed photographic image of a vibrating glottis in an in vivo canine model at closure. Note the apposition of the lower margin while the upper margin is apart.

Turn toward the midline. In Fig. 1C, the lower margins are touching at midline, while the upper margins of the folds are still apart. Further into the cycle, the upper margins will return to midline and a subsequent cycle will ensue. Figure 2 depicts a coronal section of the larynx through the midportion of the vocal folds at a point in time similar to that of Fig. 1C.

From Fig. 2, the vocal fold’s configuration can be approximated by a simplified two-dimensional traveling wave equation (Eq. 1) (7).

\[ u(x,t) = A \cos[k(x - ct)] \]  

where \( k \approx \pi/\lambda \). Depicted also in Fig. 2 are a number of terms used in Eq. 1. Lambda (\( \lambda \)) is the wavelength of the vocal fold or the effective vibratory distance from inferior to superior. \( A \) is the maximum amplitude of vibration, \( u \) is the vocal fold’s transverse or lateral displacement at any particular vertical distance \( x \). Variable \( k \) is defined as the wave number and refers to the number of wavelets in one cycle (7). For the case of the vocal folds, \( k \) is less than 1 and may approach \( 1/4 \) (I. Titze, unpublished observation). In Eq. 1, \( c = \) velocity of the wave in the \( x \) direction, also called wave speed or phase velocity. The term phase velocity is used because points of equal phase travel at the same velocity. It can be seen from Eq. 1 that the displacement at any vertical point \( x \) or time \( t \) is related to the product of the maximum amplitude \( A \) and a cosine term \( k(x - ct) \). Expressions that contain \( (x - ct) \) are indicative of those resembling a time harmonic or traveling wave.

Furthermore, it can be shown that the displacement velocity or particle velocity is as follows:

\[ \dot{u}(x,t) = Akc \sin[k(x - ct)] \]  

FIG. 2. Diagram of coronal section of the midportion of vocal folds and a point in the cycle similar to that in Fig. 1C.
where $A = \text{amplitude}$, $k = \pi/\lambda$ (vibrates as half a sine wave), and $c = \text{phase or wave velocity}$. Thus, the phase velocity or traveling wave speed may be one of the main controlling factors in determining the displacement velocity. Also, note that if $c$ is directly proportional to the product of the wavelength ($\lambda$) and frequency, then an increase in $c$ or a decrease in $\lambda$ will produce an increase in vibration frequency. In fact, traveling wave velocity is one of the important factors controlling the fundamental frequency of phonation (8,9).

What controls the wave velocity? It can be shown that the wave velocity ($c$) in any viscoelastic medium such as the vocal folds is related to the following equation (10):

$$c = \sqrt{\frac{\text{(resistance to deformation of the medium or } E)}{\text{(density)}}}$$

where the elastic modulus ($E$) is defined as follows:

$$E = \frac{\text{(force required for displacement)}}{\text{(area to which the force is applied)}}$$

$$E = \frac{\text{(change in length at a particular length)}}{\text{(change in length at a particular length)}}$$

In summary, the displacement velocity is proportional to the wave speed, which is in turn proportional to the elastic modulus of the vocal folds or vocal fold stiffness.

To understand how the stiffness of the vocal folds is controlled, we must examine the intralaryngeal and extralaryngeal innervation of the larynx. Intralaryngeally, as the recurrent or inferior laryngeal nerve enters the larynx posterior to the inferior cornu of the thyroid cartilage, it immediately divides into a posterior division that produces glottal dilatation and an anterior division producing vocal fold adduction (11). The proximal portion of the anterior division goes on to innervate the lateral cricoarytenoid and interarytenoid muscles, which produce glottal closure. The more distal portion of the anterior division innervates the thyroarytenoid muscle (Fig. 3). The thyroarytenoid muscle runs beneath the lamina propria from the vocal process to the anterior commissure. The thyroarytenoid muscle is one of the major factors in controlling the elastic modulus of the vocal folds (12). Figure 4 is from an in vivo canine experiment (13) in which the transverse elastic modulus (i.e., measured horizontally along the medial-lateral plane) of the vocal fold was measured for increasing recurrent laryngeal nerve (RLN) and superior laryngeal nerve stimulation. Because the footplate positioned against the medial edge of the vocal fold contacted the full width of the vocal fold, the elastic modulus represented the stiffness of the mucosa, ligament, and muscle of the vocal fold. As depicted, increasing stimulation produced an increase in the fold's elastic modulus.

The extralaryngeal innervation also influences the total elastic modulus or stiffness of the vocal folds. The superior laryngeal nerve external branch runs posterior to the thyroid ala to innervate the cricothyroid muscle, producing a stretching and...
thinning of the vocal folds. As shown in Fig. 4, this has the direct effect of increasing the elastic modulus of the lamina propria and secondarily acts synergistically with the thyroarytenoid muscle to further increase its effect on the elastic modulus. Finally, vocal fold thinning produced by cricothyroid muscular contraction changes the geometry of the vocal folds, producing a decrease in the wavelength of vibration and also a decrease in the amplitude of vibration (14). Thus, the strong influence of cricothyroid contraction on pitch is probably related to its effect on increasing the elastic modulus and decreasing the vibratory wavelength, i.e., \( c \) is proportional to \( \lambda \cdot f \).

While thyroarytenoid and cricothyroid muscle activation are synergistic at low to moderate levels of activation, there is some evidence to suggest that high levels of thyroarytenoid muscle activation may be antagonistic to cricothyroid muscle activation and reduce the stiffness of the vocal fold (15). In a system as specialized and complex as the larynx, many other factors also come into play that alter vibration. For example, the amplitude of vibration is quite variable and is influenced by a number of factors such as air flow rate, cricothyroid and vocalis contraction, and vocal tract configuration. Furthermore, the vocal folds’ elastic modulus will be different depending on whether the transverse, longitudinal, or shear modulus is being measured (anisotropy). Also, because of this anisotropy and energy dispersion, the wave speed may not be constant but may vary from the lower to upper vertical extent of the folds (6).

One means of gaining further insight into the biomechanics of laryngeal vibration is by examining the effect of pathologic states on that vibration. For example, if, as stated earlier, the displacement velocity is related to the wave speed, which is proportional to the elastic modulus or stiffness, then a unilateral decrease in the stiffness would be expected to produce a unilateral decrease in the traveling wave velocity and vocal fold displacement. This type of effect would be observed in patients who exhibit paresis or paralysis of the vocal folds. Unfortunately, the two vocal folds interact during vibration and so the effect of vocal fold entrainment has to be considered whenever examining the effect of asymmetric pathologic states on bilateral vibration. Entrainment refers to those factors that produce the simultaneous opening and closing of both vocal folds. In general, entrainment occurs through tissue proximity during vocal fold opening and aerodynamics during vocal fold closing. For example, regardless of which vocal fold’s traveling wave is traveling with greater velocity, both folds move laterally in glottal opening, and conversely, both the folds move medially in glottal closing. Therefore, differences in velocity of displacement can usually only be observed when the vocal folds are not touching (i.e., during the open portion of a glottal cycle).

Let us first consider a unilateral paralysis when vocal fold closure is adequate, that is to say the vocal folds touch one another during each glottal cycle. A unilateral paralysis should produce a unilateral decrease in stiffness, slower traveling wave velocity, and less displacement from midline when compared to the normal fold. However, because of entrainment, differences existing in wave speed between the left and right vocal folds will be manifested only during the open interval. The net effect will be that the apparent displacement or vocal fold excursion will be as if the normal fold is greater than

FIG. 5. Digitized most-open and most-closed portions of videostroboscopic images from a subject following injection of Xylocaine into the left recurrent laryngeal nerve to produce a left cord paresis.
the paretic fold. Figure 5 is from a subject who underwent Xylocaine injection of his left recurrent laryngeal nerve to produce a temporary left vocal fold paresis. The digitized video images are from the most open and most closed portions of a video-stroboscopic cycle. The excursion of each vocal fold was obtained by subtracting the vocal fold width in pixels during complete closure from the vocal fold width during maximal opening, in this case, \(a - c\) on the right and \(b - d\) on the left. The \(a - c = 6\) pixels and \(b - d = 3\) pixels, indicating that the paretic left-sided vocal fold moved only 50% of the right normal vocal fold.

Using objective analysis of this type, similar findings can be observed in nearly all patients with vocal fold paresis and paralysis. These results can be interpreted as differences in traveling wave velocities manifesting as differences in displacement velocities as discussed earlier (Eq. 2). Furthermore, the asymmetries in wave velocities and vocal fold displacements affect the physical characteristics of the air flow pulses (smaller speed quotient, greater open quotient, and steeper spectral slope) and thus the acoustics and perceived quality of the sound produced (a breathy voice) (16).

A second example is a patient in whom glottal closure is inadequate, in which the vocal folds seldom touch during a vocal cycle. In this circumstance, entrainment may occur through aerodynamics only and differences in the wave velocities can be manifested during both opening and closing portions of the cycle. These types of asymmetries are observed in patients who exhibit diplophonia (17) (phonation with two simultaneous fundamental frequencies). Figure 6 is a fast Fourier transform (FFT) from a patient with diplophonia. It can be seen that there are two distinct fundamental frequencies. The next, Fig. 7, shows the characteristic photoglottographic, electroglottographic, and acoustic waveforms obtained from this patient. The electroglottography, displayed as increasing impedance toward the top, demonstrates that the vocal folds touch infrequently. Photoglottography shows the characteristic frequency-modulated-type signal often observed in these patients (18), indicating a complex vibratory pattern interpreted as limited entrainment associated with asymmetric stiffness and two different traveling wave velocities. These are just two examples indicative of the subtle relationships that vocal fold stiffness, entrainment, and degree of vocal fold closure can form in determining complex vibratory patterns and altered vocal quality.

CONCLUSIONS

Vocal fold stiffness or its manifestation (traveling wave symmetry) is an important consideration in procedures designed to restore voice. Surgical voice restoration procedures must consider the fundamental biomechanics of the larynx. Their consideration will permit modification of the individual elements controlling phonatory function.

Acknowledgment: This research was supported by NIH/NIDCD grant RO1 DC00855-01 and Department of Veterans Affairs Merit Review Funds.

REFERENCES


